# PROJECT PROPOSAL TMJD Diagnostics Device

# **GROUP 5**

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#### **Executive Summary**

The purpose of this project is to develop a wearable device to record bruxism (tooth grinding and clenching) events and joint sounds during sleep through the use of electromyography.

Patients with temporomandibular joint disorder (TMJD) frequently engage in bruxism, which wears down the fibrocartilage disc in the temporomandibular joint leading to chronic problems. Popping and clicking sounds are audible and frequently cause significant discomfort. Patients often have a difficult time in completely opening and closing the jaw, making it difficult to adequately masticate food. Over time, the condition may worsen and pain may develop in the temporomandibular joint region. TMJD often goes unnoticed until the fibrocartilage disc is finally worn down to the point where the symptoms become self-evident.

Current screening methods are ineffective at diagnosing this condition. This project is an improvement on current screening methods by allowing the patient to wear a comfortable device in their home environment and acquire data consistent with their natural sleeping habits.

#### 1. Introduction

#### 1.1 Background

Temporomandibular Joint Disorder (TMJD) affects approximately 35 million people in the United States. It can cause problems with eating, drinking, swallowing, talking, making facial expressions, and even breathing in people who suffer from it. Bruxism can wear down the fibrocartilage discs in the jaw, which makes it difficult to open and close the mouth. Bruxism, the act of grinding or clenching of the teeth, is a common symptom of TMJD that clinicians use to diagnose it.

Currently patients who are suspected to have TMJD or exhibit signs of bruxism through wear on the teeth are subject to spend a night in a sleep lab, in which they are connected to electrodes while sleeping. Those electrodes are connected to machines through wires that record and analyze the activity of the masseter and temporalis. A trip to the sleep lab is inconvenient for many patients, many of whom also have sleep apnea and typically use a breathing machine.

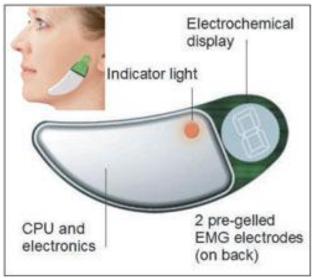
#### 1.2 Purpose of the Project

The TMJD Diagnostics Device aims to make sleep labs for TMJD diagnosis superfluous. It will make it possible for the muscular activity associated with bruxing to be recorded in the patient's home. This would take the necessity of transporting a breathing machine out of the diagnosis of TMJD for patients with sleep apnea, and be more cost effective for patients as well as their insurance companies.

# 1.3 Previous work done by others

#### 1.3.1 Products

A current low-cost bruxism diagnostic device is in the market. The BiteStrip is a single-use disposable device used by the patients at home. It is a miniature electronic system consisting of: two pre-gelled skin EMG electrodes and an EMG amplifier, for acquiring nocturnal EMG signals from the masticatory muscles; a CPU for running real-time software that analyzes EMG strength patterns and for detecting and counting each bruxing episode; a permanent chemical display for presenting the study outcome in the morning and a lithium battery. All the elements are integrated onto a small lightweight plastic film that is attached to the patient's cheek.



Components of the BiteStrip

Its indications correlate well with comparable indications from formal sleep lab studies. It is available through health providers worldwide at a very low price to the public as a self-administered or prescription test. Relevant patents were applied for, and clinical studies are in process in well-known sleep labs to prove its accuracy.

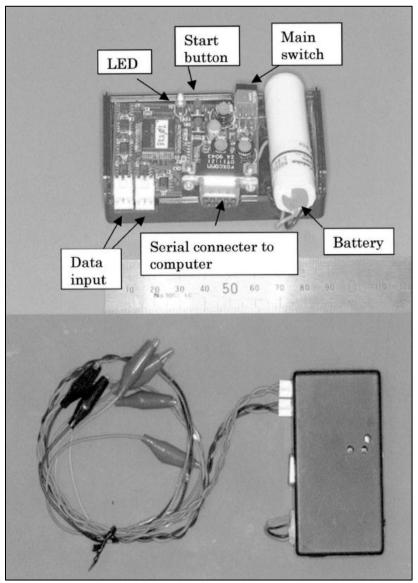
In using Bitestrip, the patient is required to perform at least two maximal voluntary clenches during the first 30 minutes by biting on a wooden spatula provided in order to establish the threshold which is set at 30% of the average EMG amplitude. The BiteStrip counts each EMG peak stronger than the threshold for a period of up to six hours. The patient then returns the Bitestrip to the clinician for interpretation of the results.

Despite the advantages offered by Bitestrip, the device presents some limitations. In the first place, the study requires a minimum of 5 hours. If the Bitestrip is removed earlier than this minimum period, an error will occur. Moreover, this device does not save the EMG signals, which may be useful for the clinician in order to assess an accurate diagnosis. Bitestrip only provides the number of bruxing events. This information will not allow the clinician to distinguish between teeth grinding and clenching, nor record the intensity of the clenching or grinding or the time when these events occur.

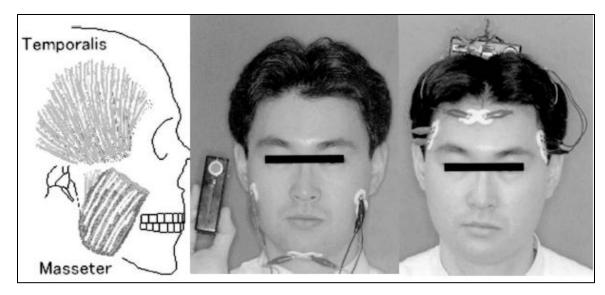
Sakagami, Horii, Ino, Matoba, Kato and Kawanami developed a portable nocturnal bruxism monitoring and analysis device in 2002 and verified its accuracy and easiness of use. Their bruxism diagnostic system consisted of two parts: the portable bruxism monitoring and analysis device, and the software that was installed to a computer.

The monitoring and analysis device (Morita MFG) was equipped with a microcomputer to autoanalyze the data. Due to the small size of this device and its light weight, it could be either placed on the forehead, or inserted in a pocket of a jacket. The device had two sets of data import connectors for pickup cables, which were hooked to the disposable electrodes (Duotrode<sup>®</sup>, Myotronics Inc., USA) attached either to both sides of the cheek over the masseter muscles, or to both sides of the temple over the temporalis muscles. In order to launch the device, the user would push the start button on the side of the device. After amplification and processing of the EMG signals, these were compared to a manually set threshold level. The device provided the total number of bruxing events as well as the lasting time of each bruxing event. Finally, the recorded data was transmitted into the computer via serial port. The device was equipped with EEPROM and the data is recorded on the memory to the maximum of 676 data sets in one night.

Although the authors who carried out the study verified the accuracy of the device, and the subjects of the study declared that it was easy to use, this device does not provide comfort and mobility to the patients due to the presence of wires. Moreover, serial communication limits the speed of data acquisition.



*Components of the bruxism monitoring and analysis device developed by Sakagami, Horii, Ino, Matoba, Kato and Kawanami.* 



**Left:** The temporalis and masseter muscles. Center: Electrodes attached to the cheek for the data acquisition from the masseter muscles, and to the chin for earthing. **Right:** Electrodes attached to the temple for the data acquisition from the temporalis muscles, and to the forehead for earthing.

#### 1.3.2 Patent search results

The Bitestrip described above has applied for relevant patents and clinical studies are in process in well-known sleep labs to prove the accuracy of this device.

In addition, after patent search, only one more device was vaguely related to the purpose of our project. It is a "Measuring device for quantifying the severity of bruxism", US patent #5,911,576, comprising of a thin shell formed to the shape and elastically retained to one or more teeth. The shell consists of many layers of different colors. The outer layer of the shell, when worn out by clenching and grinding, reveals an inner layer. This way, the regions of wear may be analyzed to determine the extent of the bruxing activity. However, this device does not provide the EMG signals for accurate diagnosis and may not be comfortable to use since it may interfere with normal breathing.

#### 2. Project Description

#### 2.1 Objective

The TMD Diagnostics Device utilizes electromyography (EMG) to obtain biosignals from the muscles involved in mastication, including the left and right temporalis muscles, and the left and right masseter muscles. These EMG signals will be used to determine if the patient is bruxing or clenching

during sleep, two major contributing factors to temporomandibular joint disorder (TMD). EMG is currently utilized in TMD sleep studies with significant efficacy in determining bruxing events. However, sleep studies are expensive and uncomfortable for the patient, resulting in data that is inconsistent with their sleep habits. This device allows the patient to perform a comfortable EMG study in their home environment and acquire accurate data.

The signals will be obtained from reusable electrodes without the use of adhesive gel, providing a superior level of comfort for the patient. The setup process is simplified by using these electrodes, allowing the user to slip the device on and make minor adjustments to ensure optimal fit, without individually attaching each adhesive electrode. The electrodes will also not have to be interchanged after each use, thus simplifying the maintenance of the device.

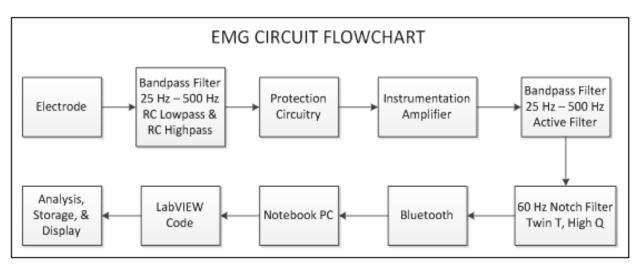
The device will be comprised of a wearable hat-like apparatus. The reusable electrodes will be securely placed inside the device over the muscles of mastication. The electrode leads will be connected to the internal circuitry so that no wires are exposed. The circuit will be enclosed and located on the top of the device so that the patient does not damage it during sleep. Both the electrodes and the circuit will be removable so that the patient can wash the exterior case. The device will be comprised of fleece to increase the comfort for the patient. Velcro<sup>®</sup> will be utilized to allow for minor adjustments and achieve an optimal fit.

The EMG signals will be sent wirelessly to a notebook personal computer. A LabVIEW program will automatically load each time the computer is powered on. The interface will be easy to use and will provide sufficient help information in addition to a detailed user manual. The user will simply run the program and initiate the data acquisition process. The program will have the capability to analyze, send, store and display data. The raw data will be processed into useful diagnostic information that may be presented to the clinician.

Wireless communication (Bluetooth<sup>®</sup>) between the device and the notebook personal computer is part of the optimal design, because it reduces the complexity of the device and also improves the patient's comfort while sleeping. The device will contain an additional serial (RS-232) port, providing an optional connection that is compatible with numerous computer configurations, not just computers with Bluetooth<sup>®</sup> connectivity. The selected notebook computer will have both Bluetooth<sup>®</sup> connectivity and a serial port to account for this. In order to test the device, subjects with TMD and control subjects will be employed in clinical trials. Therefore, an institutional review board (IRB) must be applied for in consideration of clinical trials. This will be possible with the help of the UConn Health Center and School of Dentistry.

#### 2.2 Methods

Electromyography will be used to obtain physiological data from the muscles of mastication and therefore proper analog circuit design is necessary for the successful operation of the device. Electrodes specifically designed to obtain EMG signals will be connected to an enclosed circuit represented by the flowchart below.



# EMG circuit flowchart

The frequency range of interest for electromyography is between 25 Hz and 500 Hz, with amplitudes from 100  $\mu$ V to 90 mV. However, the use of surface electrodes (surface electromyography) can decrease the signal amplitudes to a maximum of 1 mV. Taking these parameters into consideration, it is possible to design a circuit that conditions and amplifies the biological signals of interest.

An RC lowpass and RC highpass combination to form a bandpass filter is necessary for each electrode to remove unwanted frequencies that will cause distortion. The cutoff frequency for the highpass filter was chosen to be 25 Hz, but may be reduced to around 15 Hz to allow more low frequency EMG signals to pass. Likewise, the lowpass cutoff frequency for the lowpass filter was chosen to be 500 Hz, but it may be increased to pass higher frequency signals. A one-pole RC filter was chosen

here to reduce the amount of integrated circuits necessary for active filters. Each muscle requires two electrodes, thus there would need to be at least eight operational amplifiers to provide the filtering capabilities. Since space is a design constraint, RC filters are sufficient at this point in the circuit, as more filtering can be done after amplification and in the LabVIEW program as well.

Protection circuitry is an absolutely critical portion of the design of the overall device, since numerous electrodes will be attached to the patient during sleep with the potential for electrical shock. Diodes are excellent for simple protection against small voltages. Low leakage diodes will be constructed in parallel so that if the voltage near the electrode ever reaches 700 mV, the diodes will reverse and forward biased, allowing the potentially harmful current to run directly to ground. Electromyography voltages typically do not exceed 200 mV, however it is still important to protect the patient against any possibility of electrical shock.

An instrumentation amplifier was chosen as a means of amplifying the signal due to several reasons. The input impedance of a three-stage instrumentation amplifier is very high, which is desirable that minimizes loading effects. The output impedance is low with respect to the input impedance, another desirable characteristic. The gain of an instrumentation amplifier can be adjusted simply by changing one resistor value, allowing for a flexible gain factor that can be adjusted accordingly. The design also incorporates a high common-mode rejection ratio (CMRR), which is a desirable characteristic when dealing with biological signals. The AD620 instrumentation amplifier from Analog Devices is initially selected since it provides a superior performance to the classic three-stage instrumentation amplifier, has a gain adjustable from 1 to 10,000 by changing one external resistor, exhibits low noise (280 nV p-p noise from 0.1 Hz to 10 Hz) at a frequency below that of the EMG signals. It is specified on the manufacturer's data sheet that it is applicable to ECG and medical instrumentation, and works well with battery operation and portable equipment, with a maximum supply current of just 1.3 mA. Because the AD620 has the three-stage instrumentation built into a small package, it saves space on the printed circuit, which is another desirable parameter for consideration.

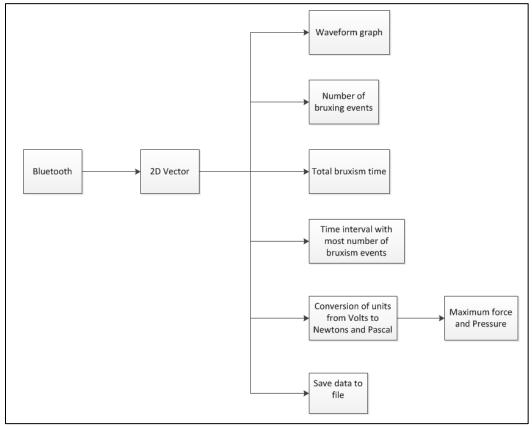
An active bandpass filter following the instrumentation amplifier is implemented in the design to further suppress frequencies outside of the EMG signal range. An op amp design will be used to provide for a higher order circuit with a high Q-factor. Constructing the filter circuit after the instrumentation amplifier also allows for the suppression of noise created by the previous electrical components. It is desirable that the operation amplifier used for filtration does not introduce noise, thus a low-noise op amp will be selected. A quad amplifier will be utilized to save space on the printed circuit board and eliminate the need to have four separate op amps. This configuration will also reduce the noise of the circuit because it eliminates cross-talk between multiple op amps and noise introduced from other components utilized in the filter design. The LM3900 by National Semiconductor was selected because it meets all of the design parameters and is a low cost quad operational amplifier.

A 60 Hz notch filter with a twin T design will be implemented to remove power line interference. This design has a high Q-factor and an infinitely deep notch, ensuring that only 60 Hz noise is filtered. Since this is part of the EMG signal bandwidth, proper design of a notch filter is necessary to ensure that the biological signals in the lower frequency range are not suppressed.

Bluetooth has been selected as the communication protocol of choice. It allows for a wireless interface, significantly reducing the complexity of the device and making it user-friendly for set up and maintenance. Bluetooth modules can generally be powered from low voltage supplies and work excellent when powered by battery. The range can be anywhere up to 350 feet or more, which is desirable since the receiving laptop may be across the user's room. Since not all computers are compatible with Bluetooth, an additional serial port will be incorporated into the circuit so that the device can transfer data to other computers.

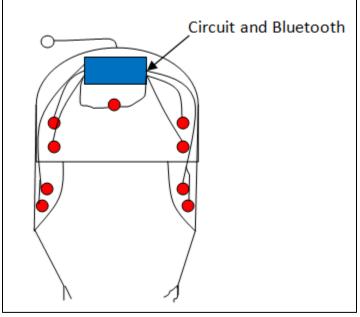
The laptop would be provided by the clinician to the patient. It should be cost effective, small size and have a light weight for easy transportation. It will also be required to have built-in Bluetooth in order to receive the processed signal from the circuit. In addition, it must meet the requirements needed to launch a LabVIEW application: operating systems Windows XP, Windows Vista or Windows 7, Pentium III/Celeron 866 MHz or equivalent, at least 255 MB of RAM memory, a screen resolution of 1024x768 pixels and 1.6 GB of disk space. The laptop will be strictly configured to be user-friendly, ensure proper functionality and prevent any modifications by the user. For example, it will be configured so that when the user turns on the laptop, the LabVIEW application will launch automatically. Also, it will prevent the user from installing or deleting applications. Ideally, the user will only have to click a Start button in the LabVIEW application to launch the program and click a Stop button at the end of the session. This will ensure an easy use of the device and prevent errors of operation by the user.

An executable file will contain a LabVIEW program in charge of performing an analysis on the data received and saving the results in a file. The program will be able to receive data from the built-in Bluetooth device of the laptop. In order to do so, a Bluetooth client application will be built in LabVIEW. To launch the program, the user will have to click a Start button. A window will pop up asking to enter the name of the file where the data corresponding to that session will be saved. The user will be required to enter the current date as the name of the file. Next, the program will initiate a loop that will constantly add the data with their corresponding time as elements of a 2D vector. As the data is being acquired, it will be continuously saved in the specified file and displayed in a waveform graph in the front panel. In addition, the program will perform analysis on the data contained in the vector. These will include calculating and displaying the total number of bruxism events detected, the total duration of bruxism events, the time interval where most number of bruxing events occur and a unit conversion from Volts to Newtons and Pascals to display then maximum force and pressure. A clear display of the data plus the additional information provided by the analysis of data will facilitate the diagnosis by the clinician. A flow chart describing the functionality of the LabVIEW code is displayed below.



LabVIEW program flowchart

The proposed product will look like a winter hat. It will house nine reusable electrodes as well as a circuit and a Bluetooth device, which will communicate with a netbook computer. The device will be comfortable and easy to use. The preliminary hat design is shown in the figure below.



Preliminary Hat Design

Once the product is completely ready for use, 20-30 clinical trials will be performed. Volunteers will be compensated at least \$100 to use the device for three nights, over which they will wear the hat product, and take home the netbook. The LabVIEW program will record the data transmitted to it by the Bluetooth device in the hat, which will further filter and analyze the data. The data will be saved automatically, so that the clinician can review the results, and determine a diagnosis.

# 3. Budget

The total budget estimated for the building of the device is \$3,770. However, due to possible errors and development costs, the final budget of the device would be reduced by approximately 65%. Excluding clinical trials from the final product cost, the final production cost would be approximately \$600. The table shown below details the cost of the various components.

Component	Maximum estimated price
Electrodes	\$50
Electrode leads	\$20
Integrated circuits	\$40
Resistors, capacitors and diodes	\$20
9 V batteries	\$10
Bluetooth module	\$100
Hat	\$30
Laptop	\$500
Clinical trials	\$3000
ΤΟΤΑΙ	\$3,770

# Budget for proposed project

The clinical trials are the most expensive component of the project because monetary compensation must be provided to the volunteer participants. A standard compensation for a clinical study is approximately \$100 per volunteer, thus with twenty to thirty volunteers the study may cost up to \$3,000.

# 4. Conclusion

The project will be beneficial to both the clinician and the patient by providing accurate data and ensuring that the correct diagnosis is realized. It is an improvement on current products in several ways. First, it eliminates the need for the patient to stay overnight in a sleep study, which is both . Second, it will be comfortable and allow the patient to obtain optimal sleep because there are no external wires and will not restrict the patient's movements. The design of the hat is unique in that it allows for repeated usage and the ability to be washed. Third, data will be acquired in the patient's home environment, ensuring that data is consistent with their natural sleeping habits. Fourth, it will display the raw electromyography data, which most current devices neglect to save. In addition to electromyography data, important diagnostic information will be presented, including the number of bruxing events, the maximum force of clenching, the time at which the bruxing events occur, and the total duration of bruxism. All of these features are vast improvements on the current techniques for temporomandibular joint disorder diagnosis.